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## Scalable Production of Highly Sensitive Nanosensors Based on Graphene Functionalized with a Designed G Protein-Coupled Receptor

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### Nanomaterials research is attracting international attention:

#### US DoD

#### Totals \$15M/year, graphene research is near 1% of DoD annual basic research budget

- •DARPA CERA Program, \$30M
- •2 Air Force MURIs, \$15M
- •3 Navy MURIs, \$22M
- •Army MURI, \$8M

 US holds 40% of graphene-related patents, trailing Asia (45%)

Patent landscape is rapidly shifting towards Asia



#### Initiating biggest research initiative ever to increase graphene IP stake (12%) $\rightarrow$  €1B (\$1.38B) over 10 years Europe – Graphene Flagship



Earliest priority filing date 2009 or earlier





China and Korea are rapidly becoming the pacesetters in terms of graphene manufacturing, packaging and integration.

> Basic research publications by China outnumber US 3:2



### Are we maximizing our return on investment?

- • Devices fall short of theoretical performance limits because of contamination issues
- • There exists variation across a single sample and batch to batch variation
- • Reproducibility and reliability are necessary for viable manufacturing process





### Variability can have a dramatic impact on device properties



Dan et al., Nano Letters (2009)



- • As an example, graphene devices used in chemical sensing applications demonstrate a false response from resist residue
- • Clean devices do not sense well, and intentionally functionalized devices function more reliably





Dankerl et al., Advanced Functional Materials (2010)

#### Epitaxial graphene, solution gated, mobility ~ 100-200 cm $^2$  V<sup>-1</sup> s<sup>-1</sup>

- • Only a handful of examples exist in the literature reporting large scale (hundreds or greater) arrays of graphene electronic devices.
- •Success in maintaining the native graphene quality is limited.

![](_page_7_Picture_0.jpeg)

## Towards Large Scale Device Manufacturing

![](_page_7_Figure_2.jpeg)

#### CVD graphene, back gated, mobility  $\sim$  700 cm<sup>2</sup> V<sup>-1</sup> s<sup>-1</sup>

- • Only a handful of examples exist in the literature reporting large scale (hundreds or greater) arrays of graphene electronic devices.
- •Success in maintaining the native graphene quality is limited.

![](_page_8_Picture_0.jpeg)

![](_page_8_Figure_1.jpeg)

#### Exfoliated graphene, back gated, mobility  $\sim$  2000 cm<sup>2</sup> V<sup>-1</sup> s<sup>-1</sup>

- • Only a handful of examples exist in the literature reporting large scale (hundreds or greater) arrays of graphene electronic devices.
- •Success in maintaining the native graphene quality is limited.

![](_page_9_Picture_0.jpeg)

# Motivation: Better Diagnostics

- • Clinical immunoassays have limitations:
	- 1)**Costly**
	- 2)Significant processing time
	- 3)Specific for a particular analyte

![](_page_9_Picture_6.jpeg)

- One sensor, one analyte•
- Best sensor available is not •technologically matched

![](_page_9_Picture_9.jpeg)

![](_page_9_Picture_10.jpeg)

![](_page_9_Picture_11.jpeg)

![](_page_9_Picture_12.jpeg)

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### Chemical Detection Platform: NanoCarbon Transistors

**Goal:** Develop a modular chemical detection platform adaptable to any vapor or liquid target with high sensitivity and selectivity

#### NanoCarbon Platform:

Transistor devices based on carbon nanotubes and graphene can be fabricated into large arrays and then functionalized with biochemical agents for tailored detection of molecules of interest.

Scalable: 100 sensors on a dime

**Modular:** Generic chemistry can be easily modified to detect any molecule

**Low cost:** Materials cost <\$0.10 per sensor

Rapid detection: Minutes

**Robust** to possible interfering compounds

![](_page_10_Figure_10.jpeg)

![](_page_10_Figure_11.jpeg)

**Sensor Fabrication:**High yield process (>98%) for making large arrays of transistors at a small size scale [1]

![](_page_10_Figure_14.jpeg)

**Sensor Operation:**

**Sensor Functionalization:**

Transistors are chemically modified to detect molecules of interest [3]

![](_page_11_Picture_0.jpeg)

-

-

 $\mathcal{L}_{\mathcal{A}}$ 

![](_page_11_Figure_1.jpeg)

Graphene field effect transistor (GFET) fabrication process:

- Graphene patterned by conventional lithography is contaminated by resist residue
- -Need a method to **pattern graphene during transfer**
- - Gold is evaporated onto the graphene using a shadowmask
- - Gold/Cu foil covered in PMMA
	- PMMA removed by bubble transfer technique
- $\rightarrow$  Uncovered graphene is removed preferentially
- Graphene strips are transferred to Pd electrodes-

Yield is >99%

![](_page_12_Picture_0.jpeg)

![](_page_12_Picture_1.jpeg)

Bubble transfer:

- • Cu/Graphene/PMMA stack is lowered into a solution of NaOH
- • There is a potential difference maintained between the copper foil and the solution
- $\bullet$  Electrochemically drives the formation of hydrogen and oxygen bubbles at the electrodes
- • Bubbles gently lift graphene/PMMA from the copper

Gao et al., Nature Communications (2012)

![](_page_13_Picture_0.jpeg)

## Electrical Characterization of Transistor Array

![](_page_13_Figure_2.jpeg)

Performance characteristics of GFETs:

- a) Representative set of 50 highly uniform I-V $_{\rm g}$  curves along with graphene FET schematic
- b) Histogram of GFET mobility
	- Average at 1500 cm<sup>2</sup>  $V$ <sup>1</sup> s<sup>-1</sup> •
- c) Histogram of GFET Dirac Voltage

•Average at 15 V

![](_page_14_Picture_0.jpeg)

#### Chemical Detection Platform: Opioid Functionalization

![](_page_14_Figure_2.jpeg)

### Tailored chemical

detection of opioids:

- a) Diazonium-based approach to chemical functionalization
- b) Activation and stabilization with EDC/sNHS
- c) Mu opioid receptor (GPCR) displaces sNHSat lysine residues
- d) Mu receptor binds target naltrexone

![](_page_15_Picture_0.jpeg)

![](_page_15_Figure_1.jpeg)

Characterization by Raman spectroscopy and Atomic Force Microscopy:

- - Raman spectra show strongly enhanced Dband (near 1360 cm-1) after diazoniumtreatment
- -Indicates the formation of sp<sup>3</sup> hybridized **carbon-carbon bonds** on the graphene surface.

AFM image of mu receptors decorating the graphene surface

Histogram of the heights of proteins indicates that the 46 kDa mu receptor monomer is ~4 nm tall on the surface, with dimers and trimers of 8 nm and 12 nm respectively.

![](_page_16_Picture_0.jpeg)

### Chemical Detection Platform: Opioid Functionalization

![](_page_16_Figure_2.jpeg)

Current-gate voltage (I-V $_{\rm G}$ ) characteristic measurements:

- a) I-V<sub>G</sub> functionalization steps at 1µg/mL <sub>G</sub> plots after successive naltrexone
- b) Naltrexone in buffer leads to an increase in the Dirac voltage of 8.5 V (green curve to orange curve).
- c) l-V<sub>G</sub> functionalization steps at 100 pg/mL plots after successive naltrexone
- d) Naltrexone in buffer leads to an increase in the Dirac voltage of 1.8 V(green curve to orange curve).

![](_page_17_Picture_0.jpeg)

![](_page_17_Figure_1.jpeg)

$$
f(C) = A \frac{C^n}{K_d^n + C^n} + Z
$$

Sensor response (increase in Dirac voltage) shows discernable signal from the bare buffer response at 10 pg/mL naltrexone.

**10 pg/mL naitrexone.**<br>The data are well explained by a<br>modified Hill-Langmuir equation<br>(black curve).<br>Tillemer et al., Nano Letters (2014

![](_page_18_Picture_0.jpeg)

### Chemical Detection Platform: Opioid Functionalization

![](_page_18_Picture_97.jpeg)

![](_page_19_Picture_0.jpeg)

## Chemical Detection Platform: Raman Readout

![](_page_19_Figure_2.jpeg)

Raman spectra during functionalization steps:

- 1) D/G ratio increased after diazonium treatment and 2D/G ratio decreased from 1.5 to 0.95
- 2) Little change between diazoniumtreatment and mu protein attachment

Upon exposure to Naltrexone, there were significant shifts in the G-peak and  $2D$ peak positions which were concentration dependent

![](_page_20_Picture_0.jpeg)

## Chemical Detection Platform: Raman Readout

![](_page_20_Figure_2.jpeg)

- a) Mu-functionalized device showing Raman G peak shift of  $\sim$ 1.5 cm<sup>-1</sup> before (green) and after (orange) Naltrexone exposure at 10 µg/mL.
	- 2D peak position shift of  $\sim$ 2 cm<sup>-1</sup> for same device
- c) For device exposed to pure buffer, G peak does not appreciably shift
- d) 2D peak position is only slightly affected by buffer exposure, shifting only 0.5 cm-1 for this device.

![](_page_21_Picture_0.jpeg)

- Many publications cite contamination as an issue in production of lithographically defined graphene devices
- Performance of complex device architectures suffer
- $\bullet$  Better understanding of the contamination mechanism and alternative fabrication procedures are needed to have graphene devices realize their ultimate potential.

![](_page_21_Figure_4.jpeg)

![](_page_21_Picture_5.jpeg)

![](_page_22_Picture_0.jpeg)

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Organizing Committee Organizing Committee

![](_page_22_Picture_9.jpeg)

![](_page_22_Picture_10.jpeg)

![](_page_22_Picture_11.jpeg)

**Thank you for your attention!**

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