

3rd International Conference and Exhibition on Orthopedics & Rheumatology

July 28-30, 2014, San Francisco, USA



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Accurate Estimation of Mechanical Load on the Musculoskeletal System Using Biomechanics Modelling

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http://neuromechanics.fmh.ulisboa.pt/

Biomechanics and Functional Morphology Laboratory





MISSION

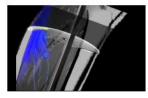
The Biomechanics and Functional Morphology Laboratory (BFML) is a research and education facility within the Faculty of Human Kinetics (FMH) and the University of Lisbon (ULisboa). It combines two areas of major international and national scientific tradition: Biomechanics and Morphological Sciences.

These two areas are dedicated to the teaching and research in Biology, Sports Science and Health Sciences. Morphology and Biomechanics are core disciplines in our undergraduate and postgraduate programs and provide an important scientific background for applications in fields such as Biology, Physical Education and Sport, Rehabilitation and Physiotherapy, among others.

The BMFL has developed an important network of collaborations with national and international reference research groups in their scientific fields, which is materialized in research projects funded (mostly under the coordination of the BMFL) and a set of doctoral or post-doctoral programs and projects.

In vivo morpho-functional evaluation using imaging techniques

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Modeling and Biomechanical Simulation of movements and muscle/joint structures



2nd Portuguese Pediatric Orthopedics Congress 2014

The LBMF, together with Prof. Elke Viehweger and Dr. João Campagnolo from Hospital D. Estefânea, participated in the 2nd Portuguese Pediatric Orthopedics Congress with a workshop entitled: "Gait analysis and its clinical use".

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Aims

Describe the integration of biomechanics experimental techniques with in vivo imaging, in order to develop subject specific models aiming at estimating the biomechanical load on the musculoskeletal system

Discuss the application of Subject Specific Musculoskeletal Modeling to Accurately Estimate Joint loading in Subjects with Knee Osteoarthritis

Address the Results After Correction of Pelvis Shape and Size and Lower Leg Muscles Insertion.





Rationale

Identification of **Gait Pattern Biomechanics** of is clearly related to Knee Osteoarthritis Risk.

Clinical Gait Analysis (CGA) is Currently used to Estimate Joint loading in Subjects with Osteoarthritis and in Particularly **Knee Adduction Moment of Force (KAM)** is Considered a Marker for Medial Compartment OA Severity.

Commonly Biomechanical Clinical Gait uses **Models Scaled Body Segments Based on Skin Markers Placement** and does not Takes in Consideration that in OA Patients with High BMI the Estimation of Joint Centers could be Severely Incorrect.

Nevertheless Joints Moments of Force estimated from CGA are used to Establish OA Risk Levels and even to Evaluate Therapeutic Intervention Programs





Overview

- Clinical Gait Analysis
- Development of 3D Biomechanics Models
 - Planar Correction of Pelvis Shape and Size (DXA)
 - Estimation of 3D Hip, Knee and Ankle Joint Moments of Force.
- Development of Subject-Specific Musculoskeletal Models
 - Estimation of Lower Limb Muscle Tension
 - Estimation of Joints Contact Forces





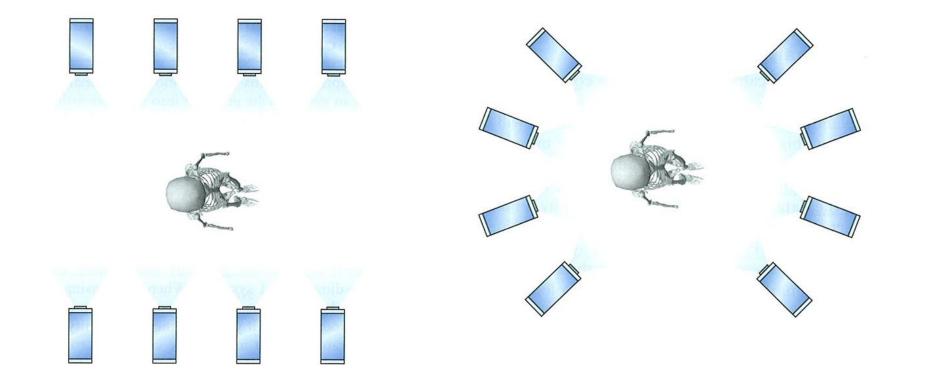
Clinical Gait Analysis Data Collection

- 1. Camera verification
- 2. Calibration
- 3. Skin marker placement
- 4. Static trial
- 5. Dynamic trial





Clinical Gait Analysis 1. Camera settings (I)





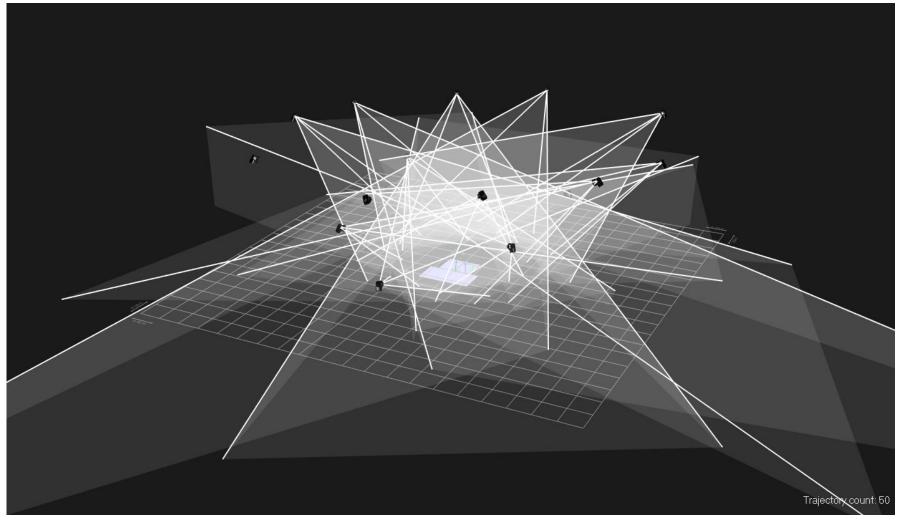




Richards, J. (2008).



1. Camera verification (II)



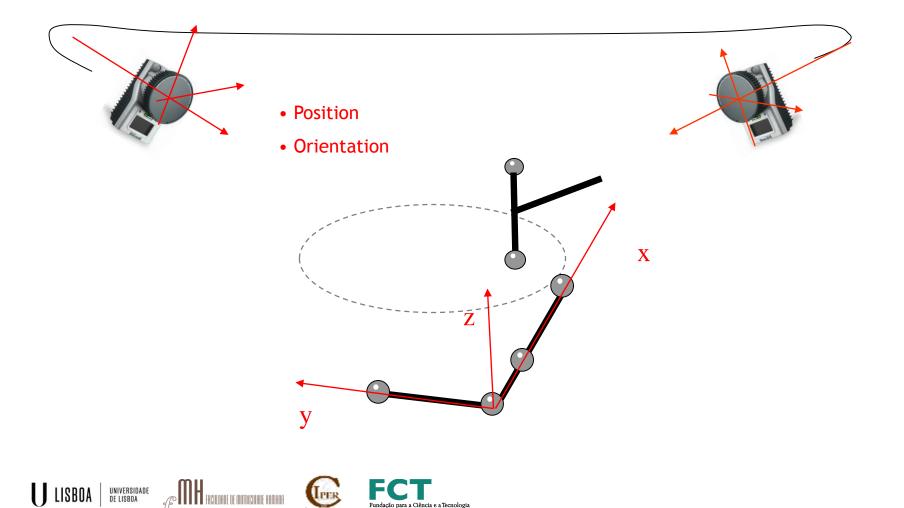
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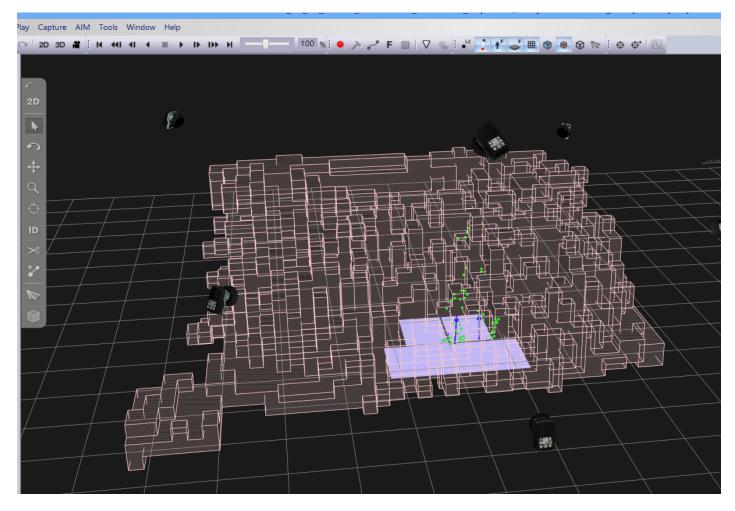


2. Calibration (I)





2. Calibration (Precision Residuals bellow 0.4 mm)

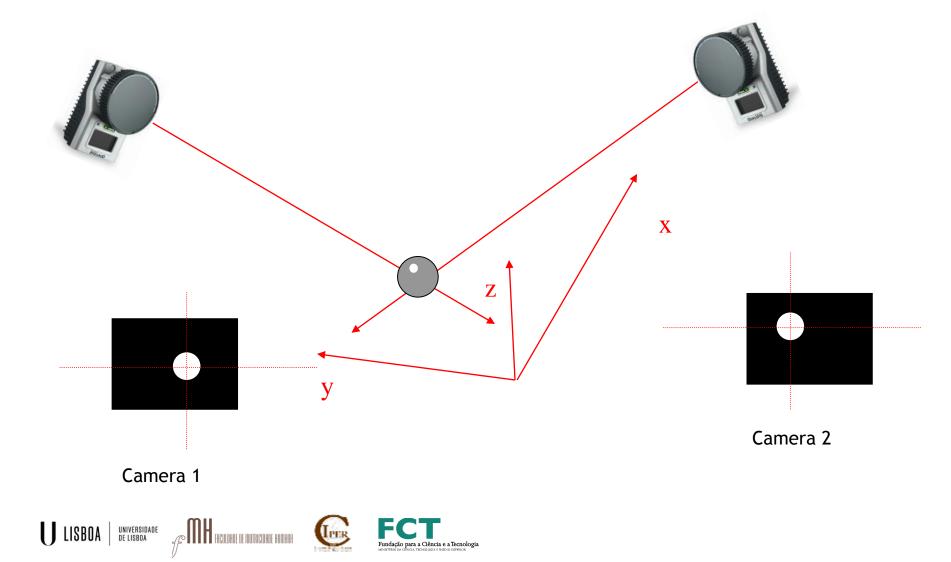






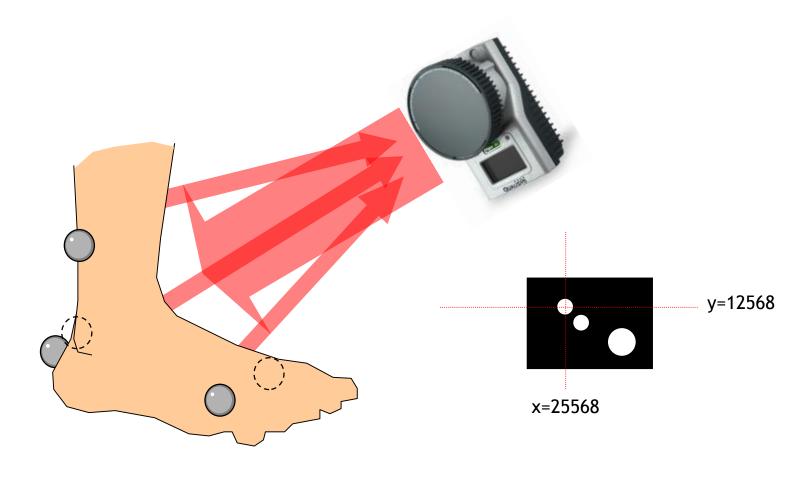








Clinical Gait Analysis 3. Marker Trajectories



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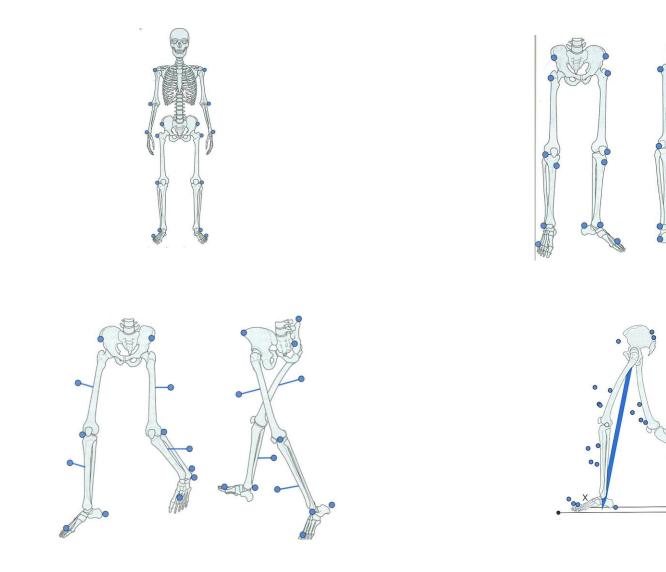


3. Skin marker placement

 $\mathcal{F}^{\mathcal{F}}$ **MH** faculdade de motricidade humana

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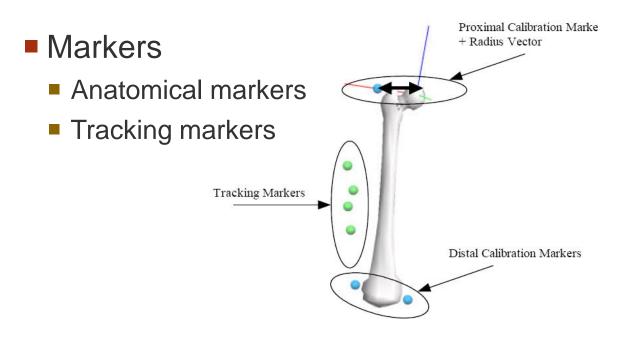
Richards, J. (2008)..

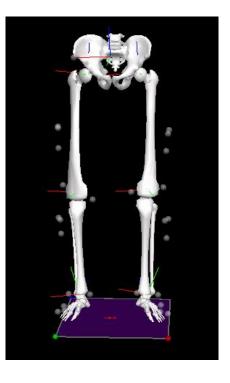
·Y



4. Static trial

Segments coordinate system definition

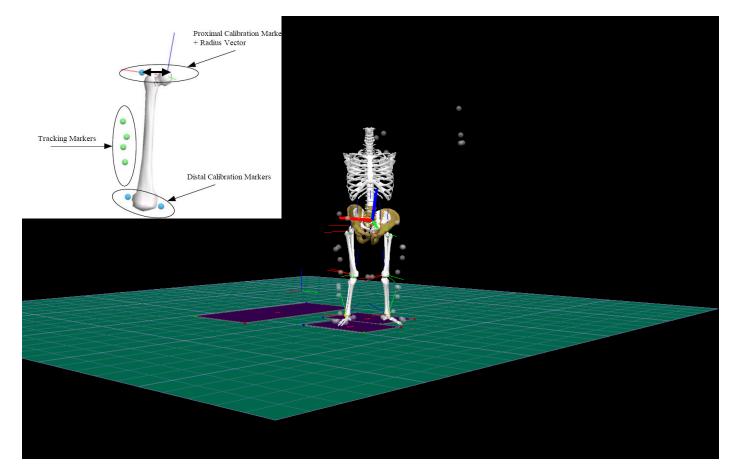








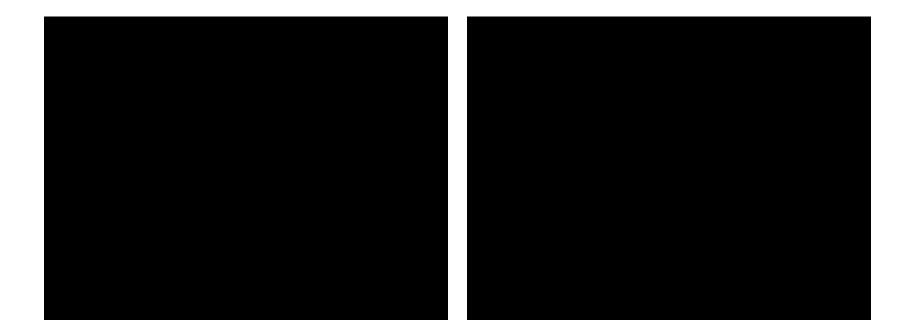
4. Static trial







5. Dynamic trial







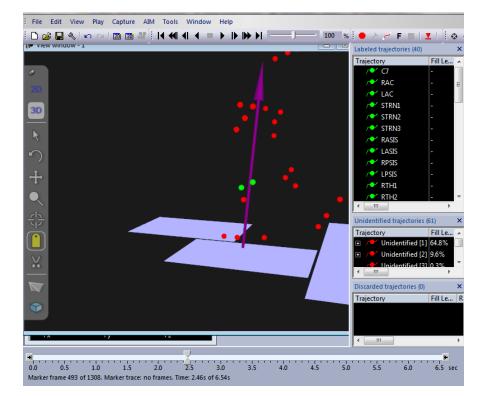


3D Biomechanics Modeling Marker Identification

- 1. Verify data quality
 - Missing or swaped markers
 - Force curves
- 2. Crop interval of interest
- 3. Identify markers
 - Label list

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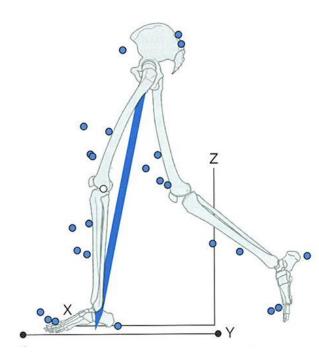
AIM model







3D Biomechanics Modeling Skin marker placement



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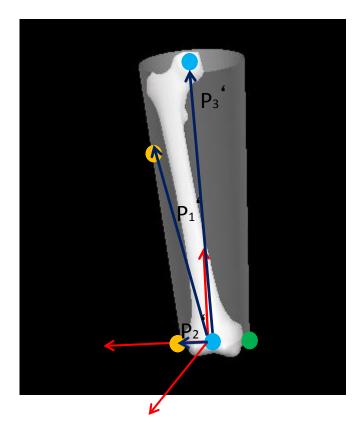
What to have in mind...

- The goals of the study
- Minimum: 3 non-collinear markers per rigid segment
- Each marker must be seen by at least 2 cameras
- The movement between the markers and the underlying bone should be minimised
- Other sensors used in the sutdy





Segment Optimization Pose Estimation Step 1: Subject Calibration



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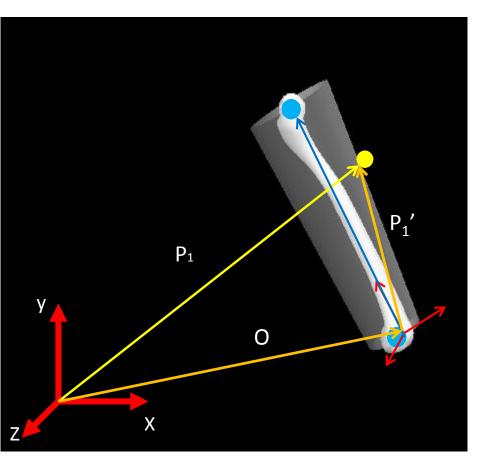
- 1. Find the anatomical based coordinate system
- 2. Find the vector (P) from origin to one of the **tracking** targets (in Lab Coordinate System)
- 3. Transform P into the anatomical coordinate system (P')

$$\overline{P}' = \boldsymbol{R}^{t}\overline{P} - \overline{\boldsymbol{O}}$$

4. Repeat steps 2-3 to find P' for all other tracking targets



Segment Optimization Pose Estimation Step 2: Motion Trial



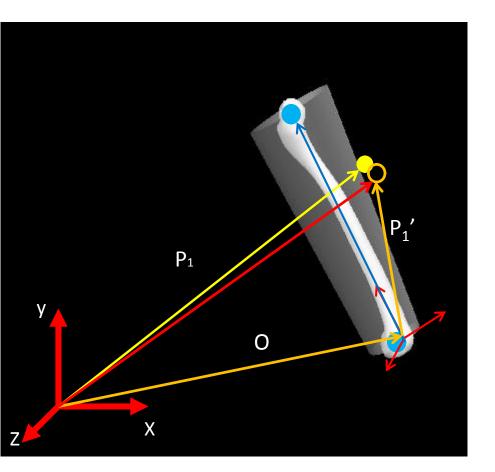
 Find the vector (P) from origin to each tracking target (in Lab Coordinate System)

- Recall the stored vector (P') from local origin to each tracking target (in anatomical coordinate system)
 - $\overline{P} = \mathbf{R}\overline{P}' + \mathbf{\overline{O}}$
- If the data was perfect:





Segment Optimization Pose Estimation Step 2: Motion Trial



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UNIVERSIDADE De lisboa If the data was perfect:

$$\overline{P} = \mathbf{R}\overline{P}' + \mathbf{\overline{0}}$$

But the data is not perfect there is an error:

$$\varepsilon = \overline{P} - (\mathbf{R}\overline{P}' + \overline{\mathbf{0}})$$

- Solve for **R** and **O** minimizing the expression: $\sum_{1}^{l} (\overline{P} - (\mathbf{R}'\overline{P}' + \overline{O})^{2})^{2}$ $I = R^{t}R$
- Under the constraint that R be orthonormal:

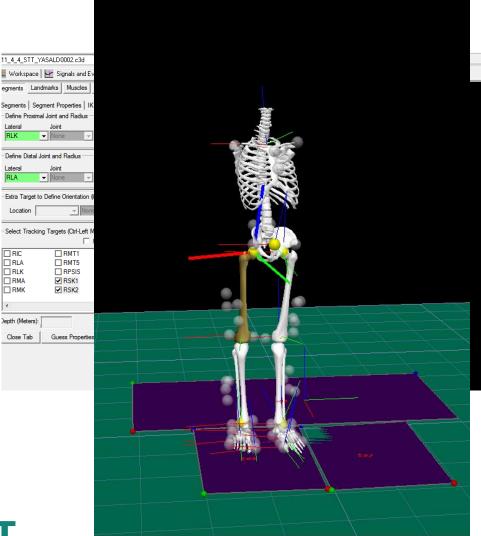


3D Biomechanics Modeling

1. Open/add c3d files

2. Create Model

3. Process/Analyse data





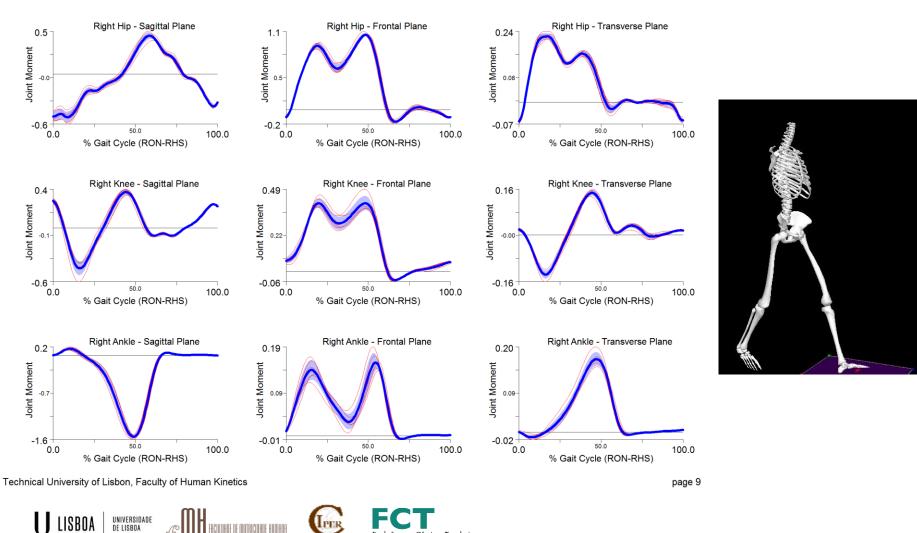




Interal

ateral

Clinical Gait Analysis Report Joints Moments of Force



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RIGHT LOWER LIMB JOINT MOMENTS

biomecânica



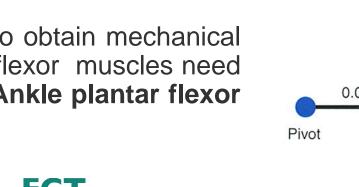
External Moments of Force

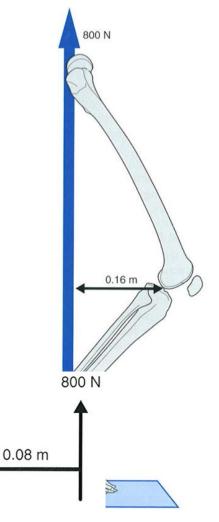
External moment of force at the ankle equal the cross product of the GRF by the moment arm of the GRF to the Ankle Joint Center. Mf ext = 800*0.08 = 64Nm

Meaning that in order to obtain mechanical equilibrium the plantar flexor muscles need to develop an internal **Ankle plantar flexor moment of force**.

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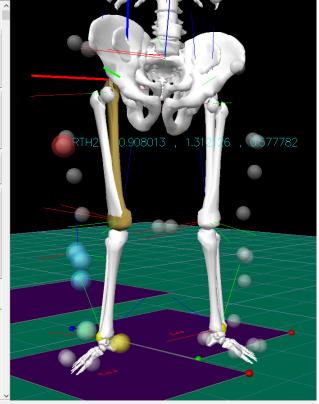




Clinical Gait 3D Segments

- Defined end points (proximal and distal)
- Local coordinate system (LCS) @ proximal end

Segments Landmarks Muscles Subject Data / Metrics								^	
Segments Segment Properties IK Constraints Right Shank									1
Define Proximal Joint and Radius									
Late	eral	Joint Center			Medial				
None		▼ R_KNEE ▼ None					-		
Radius (Meters) 0.5*DISTANCE(RLK.RMK)									
Define Distal Joint and Radius									
Late	əral		oint Cen	ter			edial		
RLA	1	 None 			<u> </u>	RMA		•	
Radius (Me	eters) 0.0	0567239							
- Extra Targe	at to Define	Orientation	(if need	ed)					
Location					~	None		~	
Select Tracking Targets (Ctrl-Left Mouse Click to Multiselect)									
Use Calibration Targets for Tracking									
RIGHT_H		R_KNEE				LAT_P		T_HIP_	
LEFT_H		L_KNEE			B_LA' RASIS			D_PSIS SACR	
Lab_x	E E	LAB_Z			LASIS			_RPV	
MID_ASI	is [PELVIS_	LAT			HIP_2		ANK	
<								>	
Depth (Meters	s):								
Close Tab	G	uess Prope	rties		A	pply	Bui	ld Model	



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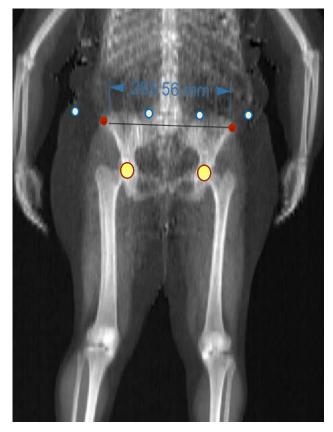


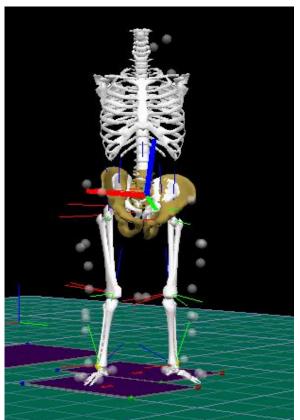


Correction of Pelvis Scaling

Development of 3D Biomechanics Models

Frontal Planar Correction of Pelvis Shape and Size (DXA)





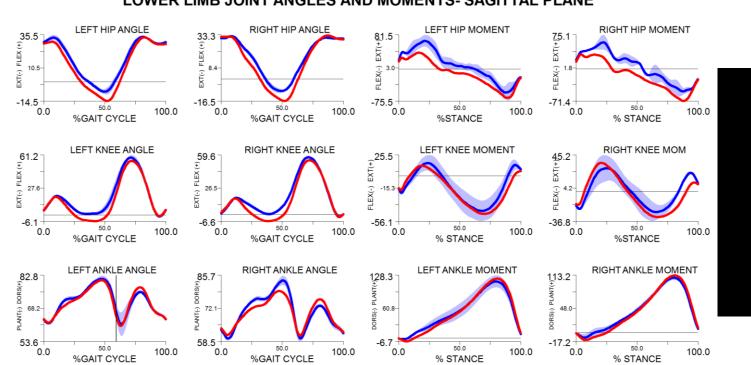




Clinical Gait Analysis Report



Corrected Versus not Corrected for Pelvis Scaling



LOWER LIMB JOINT ANGLES AND MOMENTS- SAGITTAL PLANE

NOT_CORRECTED

CORRECTED





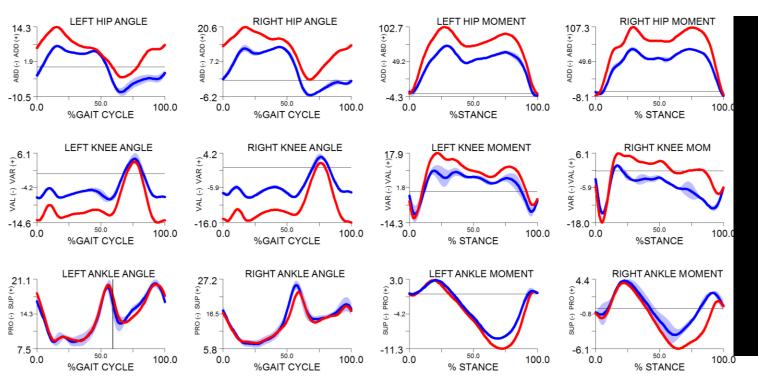




Clinical Gait Analysis Report

Corrected Versus not Corrected for Pelvis Scaling

LOWER LIMB JOINT ANGLES AND MOMENTS- FRONTAL PLANE



NOT_CORRECTED

CORRECTED

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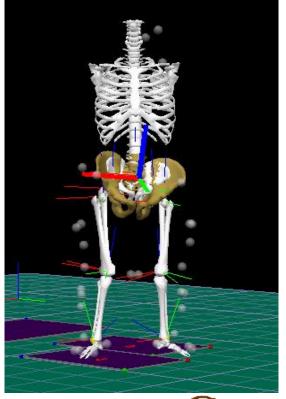


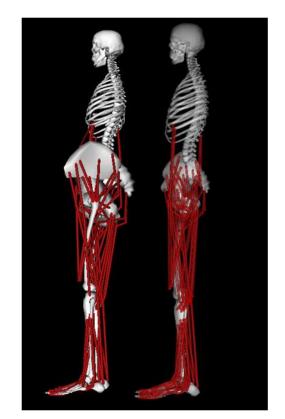


Correction of Pelvis Scaling

Development of Musculoskeletal Models

Based on Frontal Planar Correction of Pelvis Shape and Size (DXA) and Muscles Insertion correction from





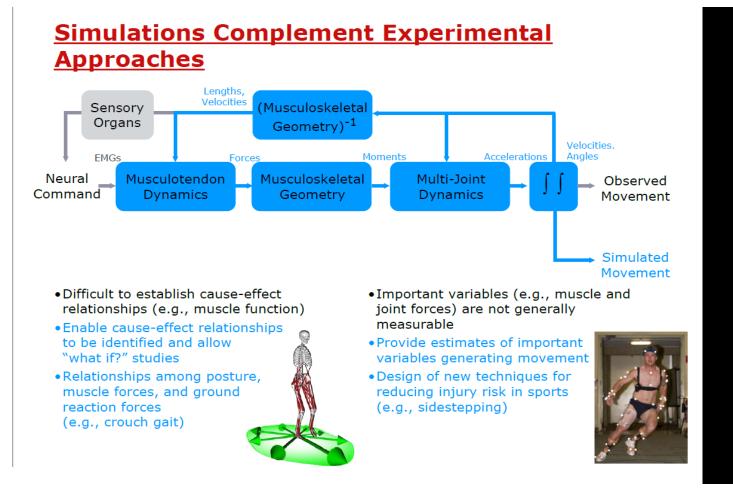
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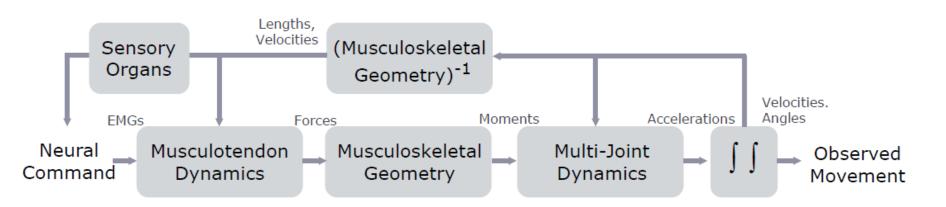


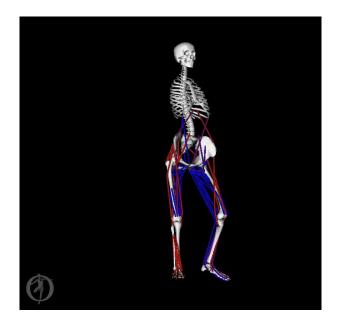
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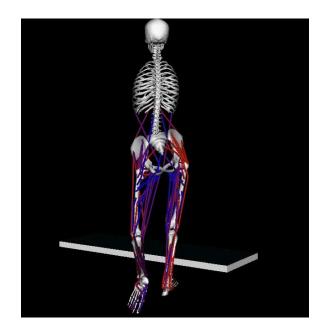


















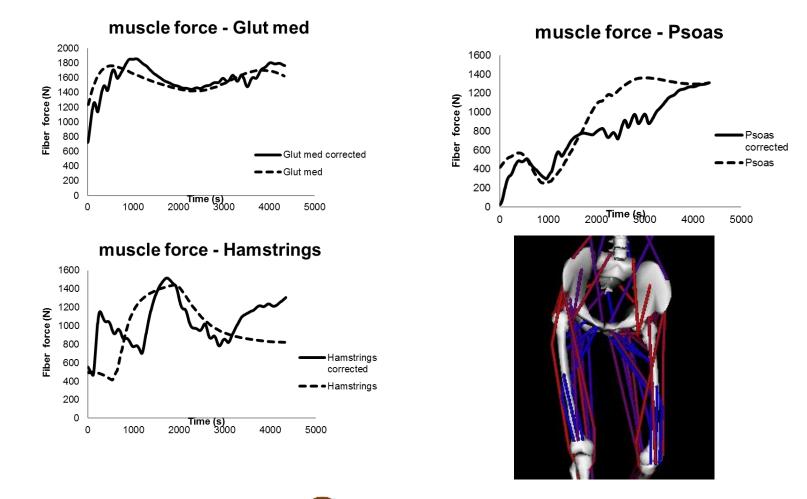
Muscle Forces

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Corrected Versus not Corrected for Pelvis Scaling

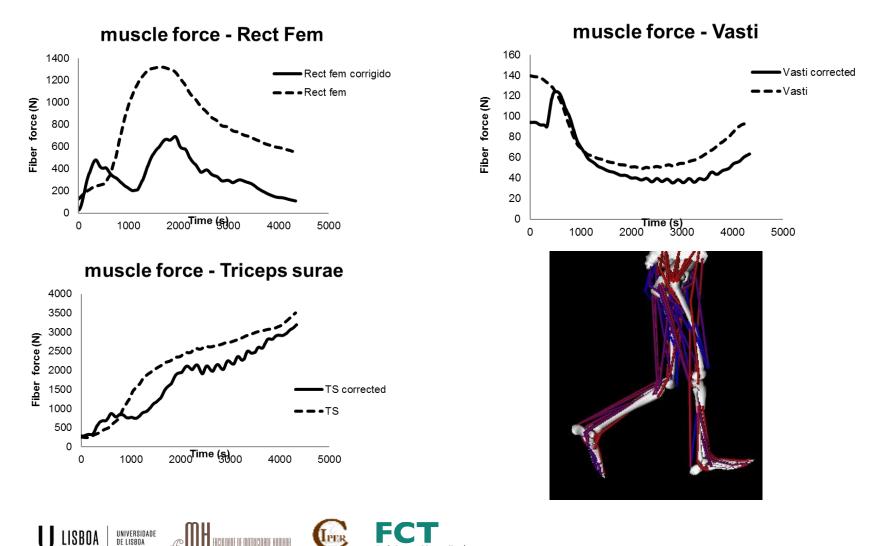


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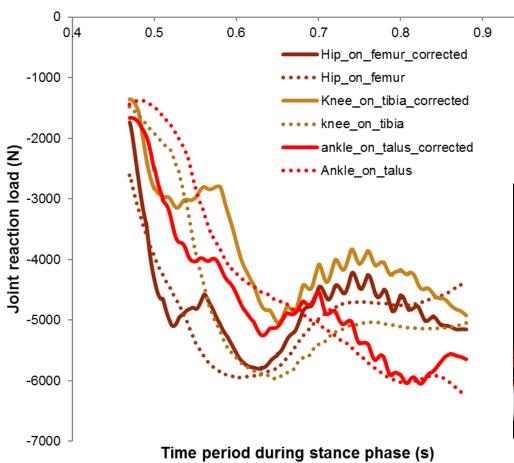
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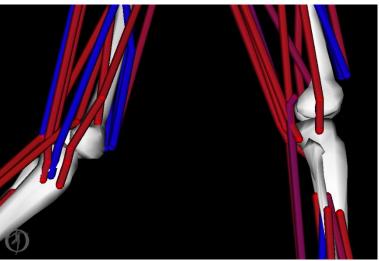
Muscle Forces Corrected Versus not Corrected for Pelvis Scaling



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Joint Reaction Forces – bone on bone with muscle action















Results

Our results showed that osteoarthritic patients that have high level of soft tissue artifacts perturbing the direct estimation of moments of force in the coronal plane that apparently are overestimated when compared with the result obtained incorporating real pelvis dimensions,

Inaccuracies resulting from non-specify musculoskeletal models will also failed to obtained correct muscle activations mainly in abductor and adductor muscles and this will lead to inaccurate estimation of bone on bone compression forces on both hip and knee joint that are severely influence by muscle tensions.





Thank you!

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• Filomena Carnide	 Filomena Vieira 	Pediatric Orthopedies Congress with a workshop entitled: "Gait analysis and its clinical use".			
• Margarida Espanha	• Paulo Armada da Silva				
 Pedro Mil-Homens 	 Ricardo Matias 				
 Rita Santos Rocha 	 Sandra Amado 				
• Vera Moniz-Pereira	• Wangdo Kim				

Group Publications - 2013/2014



Biomechanics and Functional Morphology Laboratory